

1 **Supplementary Materials: Micellar formulations of cyclosporine for ocular delivery:**  
2 **investigating micelles' penetration mechanisms for anterior and posterior segment targeting**

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4 Martina Ghezzi, Ilaria Ferraboschi, Andrea Delledonne, Silvia Pescina, Cristina Padula, Patrizia  
5 Santi, Francesca Terenziani, Sara Nicoli  
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7 **1. Analytical methods**

8 **1.1. Cyclosporine and linolenic acid quantification method**  
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10 Cyclosporine and linolenic acid quantification was performed using an HPLC-UV system (Infinity  
11 1260, Agilent Technologies, Santa Clara, CA, USA), with a reverse-phase column (Aeris™ WIDEP  
12 XB-C8 column, 150 x 4,60 mm, 3,6 μm, Phenomenex, Torrance, CA, USA) thermostated at 65°C. The  
13 mobile phase was composed of CH<sub>3</sub>CN:water with TFA 0.1% in ratio 55:45 (v/v). The flow was  
14 maintained at 1.6 ml/min and the injection volume was equal to 100 μl. The retention time of  
15 cyclosporine and linolenic acid, both quantified by UV absorbance at 230 nm, was respectively of  
16 4.9 and 3.1 minutes. Details on calibration curves, RSD%, RE% and LOQ values of HPLC methods for  
17 the quantification of cyclosporine and linolenic acid are reported in table S1. The chromatogram of  
18 a standard solution composed of alpha-linolenic acid and cyclosporine A is showed in Figure S1.  
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20 Table S1. Range of calibration curves, RSD% (relative standard deviation %) and RE% (relative error %) of cyclosporine  
21 and linolenic acid.

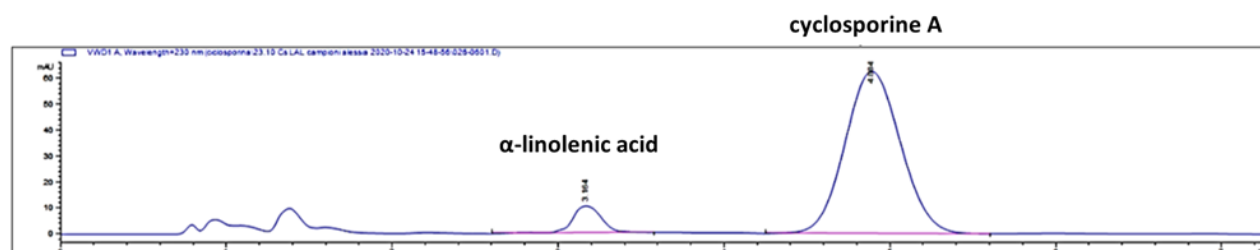
COMPOUND	CONCENTRATIONS INTERVAL (μg/ml)	RSD%	RE%	LOQ		
				LOQ (μg/ml)	RSD%	RE%
Cyclosporine	1 – 50	< 1.8	<1	1	1.2	3.2
Linolenic acid	5-100	<5.6	<5.6	5	2.3	21

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24 To determine the solubility of cyclosporine and linolenic acid in the micellar formulation, the  
25 samples were analysed by HPLC after dilution in CH<sub>3</sub>CN:water with TFA 0.1% in ratio 55:45.  
26 For the quantification of cyclosporine in the tissues, the extraction samples were diluted with water  
27 to obtain more solved chromatographic peaks. Indeed, rounded and poorly solved peaks were  
28 collected after direct injection of the extraction mixture due to the very high percentage of organic  
29 solvent (CH<sub>3</sub>CN:CH<sub>3</sub>COOH 1% in 87:13 ratio). Thus, prior to the analysis, samples were diluted by  
30 adding 60 μl of water to 200 μl of extraction sample. The same dilution was done for the preparation  
31 of the standards for the calibration curve.  
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35 Figure S1. HPLC chromatogram of a standard solution of alpha-linolenic acid and cyclosporine A at concentration 50  
36 μg/ml.

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37 **1.2. TPGS quantification method**

38 TPGS quantification was done using an HPLC-UV system (Infinity 1260, Agilent Technologies, Santa  
39 Clara, CA, USA), with a reverse-phase C18 column (Waters, Symmetry300 C18, 5  $\mu$ m, 4.6  $\times$  250 mm)  
40 and a C18 guard column (SecurityGuard Widepore C18, Phenomenex, Torrance, CA, USA),  
41 thermostated at 40 °C. The mobile phase, composed of acetate buffer pH 4.8:methanol in 3:97 (v:v)  
42 ratio, was pumped at 2 mL/min. The retention time of TPGS, quantified by UV absorbance at 215  
43 nm, was 4 minutes while the injection volume was 100  $\mu$ L. Calibration curves were built in the  
44 concentration interval 1-25  $\mu$ g/ml. For the construction of the calibration curve, a stock solution was  
45 prepared by dissolving TPGS in water at final concentration of 100  $\mu$ g/ml. The standards were  
46 obtained by diluting the stock solution in CH<sub>3</sub>CN:CH<sub>3</sub>COOH 1% in 87:13 ratio. Samples were injected  
47 without previous dilution.

48 **1.3. Sodium fluorescein quantification method**

49 The samples fluorescence ( $\lambda_{exc}$ =490 nm,  $\lambda_{em}$ =535 nm) was measured via microplate reader (SPARK10  
50 M, TECAN, Mannendorf, CH). The calibration curve was built in the range 5-500 ng/ml by dissolving  
51 fluorescein sodium in HEPES buffer. The RSD% value was lower than 4.13 while the RE% value was  
52 lower than 6.42. The LOQ was 5 ng/ml with RSD% of 0.28 and RE% of 2.21.

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54 **2. Micelles characterization**

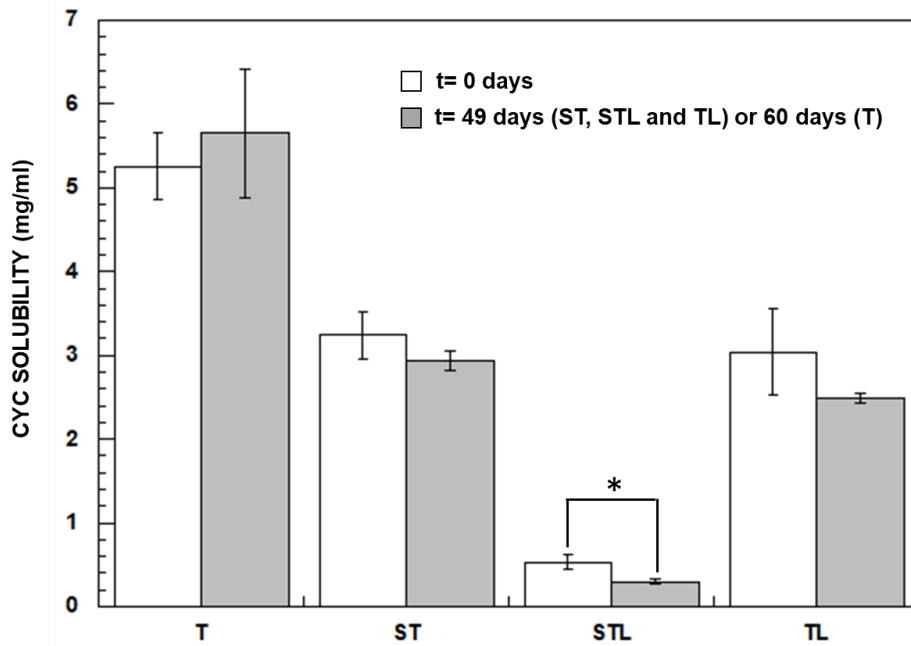
55 **2.1. Micelles size**

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57 Table S2. Size (mean  $\pm$  SD), intensity and PDI of blank and cyclosporine-loaded micelles at 0 days from preparation.  
58 Micelles were diluted 1:10 with high purity water before the analysis.

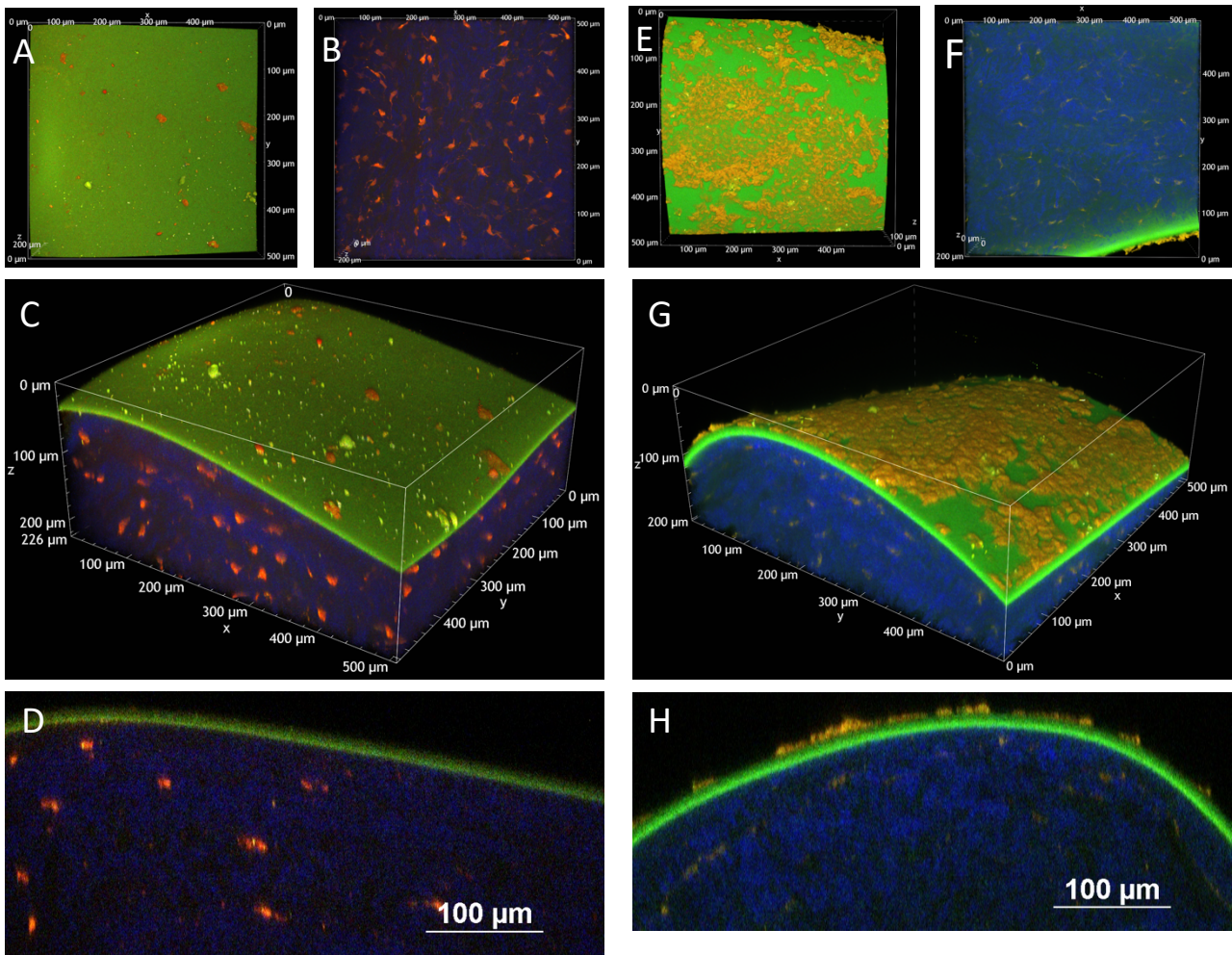
MICELLAR SOLUTION	BLANK			CYC-LOADED		
	SIZE (nm)	INTENSITY (%)	PDI	SIZE (nm)	INTENSITY (%)	PDI
S	14.09 $\pm$ 4.80	99.00	0.15	13.20 $\pm$ 2.37 444.9 $\pm$ 130.3	22.90 77.1	1.00
ST	15.10 $\pm$ 4.79	96.20	0.20	15.65 $\pm$ 5.90	94.6	0.21
T	13.86 $\pm$ 4.30 [1]	100.00	0.13	12.96 $\pm$ 4.03 [1]	100	0.09
STL	14.08 $\pm$ 3.21 341.9 $\pm$ 120.5	49.20 50.8	0.76	16.01 $\pm$ 5.88	92.5	0.23
TL	13.91 $\pm$ 3.60	72.80	0.42	14.47 $\pm$ 4.91	96.00	0.20

59 2.2. Micelles stability study



60 Figure S2. Concentration of cyclosporine in formulations T, ST, STL and TL after 0 and 49 days from preparation.  
61 Micelles T, ST and TL were stable, while formulation STL showed a significant reduction of cyclosporine  
62 concentration at 49 days. Data are reported as mean  $\pm$  SD,  $n \geq 2$ . ( $p^* < 0.05$ )  
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## 3. Two-photon microscopy

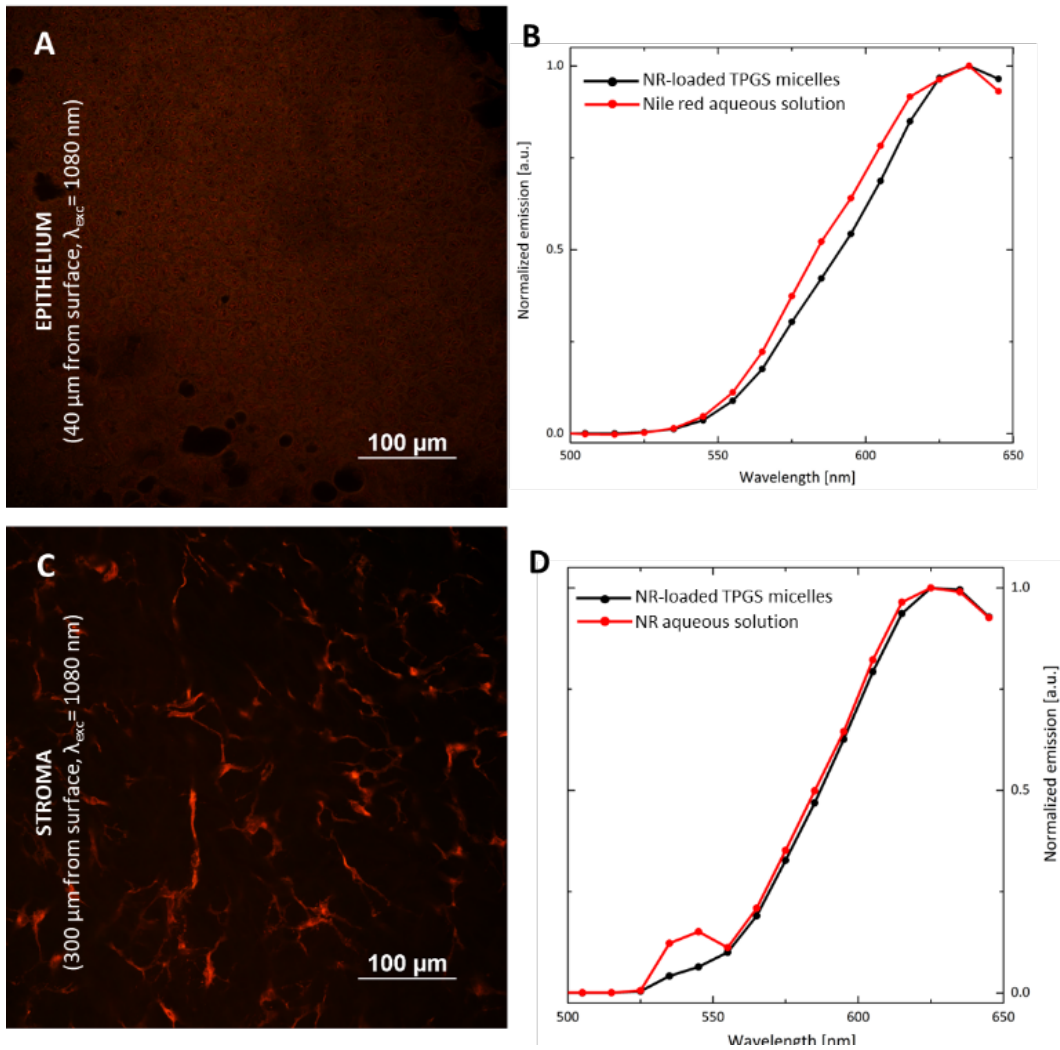


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102 Figure S3. Volume renderings of corneal tissue (endothelium side) reconstructed from Z-stack, acquired with an  
 103 excitation wavelength of 860 nm (SHG from collagen in blue, Nile red fluorescence detected in both red and green  
 104 channels). Panel A-D: sample treated with TPGS micelles loaded with NR (Z-step: 1 μm, total depth: 226 μm). Panel A:  
 105 XY view, Panel B: -XY view, Panel C: 3D overview, Panel D: XZ slice (512 μm x 226 μm). Panel E-H: reference treated with  
 106 NR aqueous solution (Z-step: 1.5 μm, total depth: 203 μm). Panel E: XY view, Panel F: -XY view, Panel G: 3D overview,  
 107 Panel H: XZ slice (512 μm x 203 μm). All the images in the two Z-scans were acquired with the same detector gains and  
 108 laser power. The thin layer characterized by a fluorescence signal which falls mainly in the green channel is the Descemet  
 109 membrane, that is usually characterized by an autofluorescence signal in the green region when irradiated at 860 nm.  
 110 Attached to this layer, some residual cells of the endothelium are present and have been clearly stained by Nile red. The  
 111 lack of integrity/absence of the endothelium can be attributed to the experimental procedure and particularly to Franz  
 112 cells dismantling, which can highly affect the fragile structure of this layer.

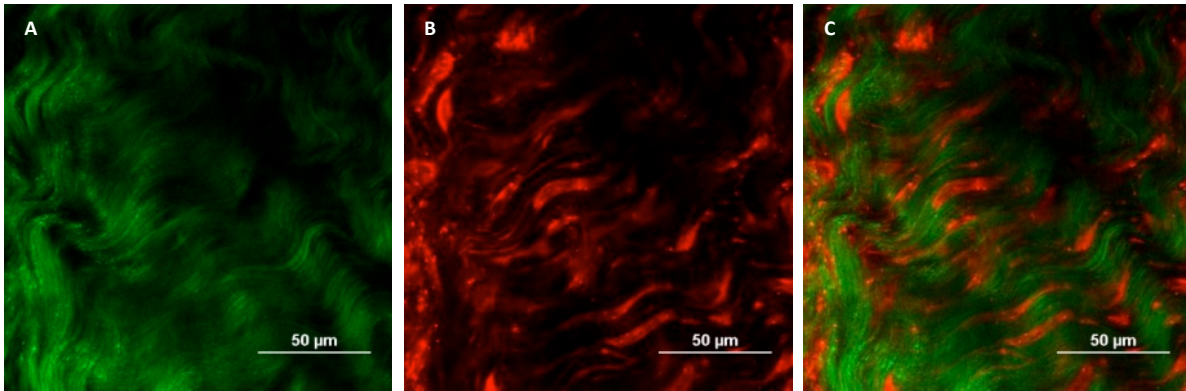
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Figure S4. Panel A and C represents respectively the corneal epithelium and stroma treated with the NR aqueous saturated solution when irradiated at 1080 nm (channels red and green channel overlay). Panel B and D shows the comparison between the emission spectra recorded in the tissue in case of the NR-loaded TPGS micelles (black line) and the reference aqueous saturated solution (red line), in the epithelium (B) and in the stroma (D) respectively. All the images have been acquired with the same detector gain for the red and green channels and same laser power. The emission profile recorded with (black line) and without TPGS (red line) micelles are almost superimposable for both epithelium and stroma indicating that the environment experienced by NR is similar in terms of polarity. In panel B, the emission spectrum of the NR aqueous solution (red line) is probably characterized by a higher contribution from the tissue autofluorescence (due to the lower Nile red concentration) that could explain the small blue-shift observed.



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Figure S5. Porcine sclera treated with NR-loaded micelles upon excitation at 1080 nm. Panel A corresponds to the SHG signal from collagen fibers (signal collected in the spectral region 510-540 nm using the spectral detector). Panel B corresponds to NR fluorescence (signal collected in the spectral region 580-650 nm using the spectral detector) . Panel C shows the image overlay: green and red images are complementary, indicating that fluorescence stems from pores inside the collagen structure and further confirming that the dye can exploit the interfibrillar matrix for its penetration.

## References

[1] S. Pescina, L.G. Lucca, P. Govoni, C. Padula, E.D. Favero, L. Cantù, P. Santi, S. Nicoli, Ex Vivo Conjunctival Retention and Transconjunctival Transport of Poorly Soluble Drugs Using Polymeric Micelles, *Pharmaceutics*, 11 (2019) 476.